

Estimating Large Lung Motion in COPD Patients by Symmetric Regularised Correspondence Fields

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Motivation and challenges for COPD registration

- 4th most common cause of death in US (caused mainly by smoking)
- Diagnosis with spirometry only global, but air trapping localised
- Ventilation of tissue quantifiable by registering exhale to inhale scan
- Strong noise in exhale scan due to ultra low-dose protocol
- Large volume differences (~100%) between inhale and exhale
- Locally varying contrast due to lung compression

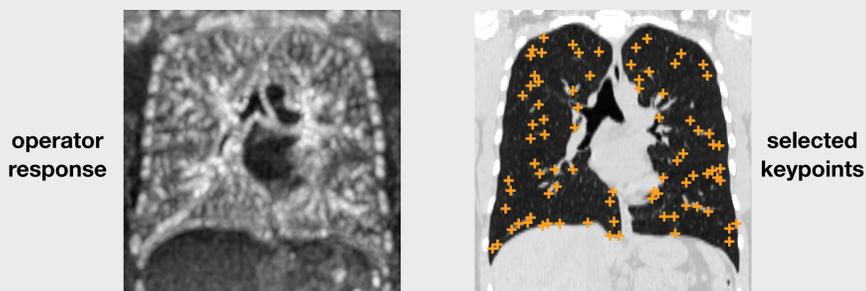
Overview of our registration approach

1. Keypoint extraction using Förstner operator (interest points)
2. Block-matching with discriminative self-similarity context [1]
3. Parts-based model [2] for regularisation + symmetry constraint

1. Keypoint extraction

- Restrict motion estimation to interesting points in image
- Förstner operator detects high local curvature (corners)

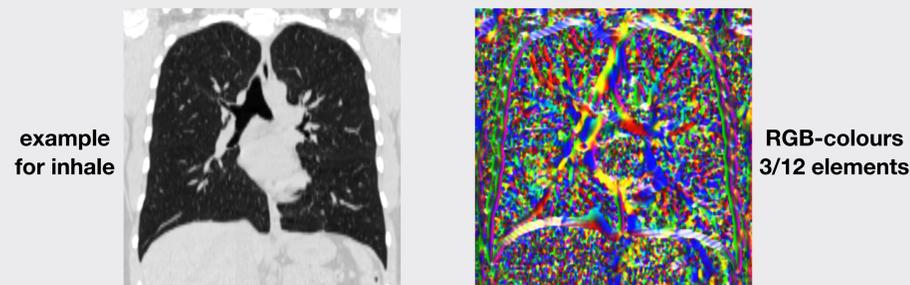
$$D(x) = 1/\text{trace}((G_\sigma * (\nabla F \nabla F^T))^{-1})$$



- Non-maximum suppression → well-distributed points within lungs
- Keypoints are only defined in fixed (inhale) scan, but dense search

2. Block-matching with self-similarity context

- Convert representation of both scans to self-similarity descriptors



- Sensitive to edges/orientation and contrast invariant
- Distance of SSC-vectors can be calculated in Hamming space
- Dense sampling of displacements and storing of all probabilities (block-matching retains only most probable vector)

$$D(\mathbf{k}, \mathbf{l}) = 1/|\mathcal{P}| \sum_{p \in \mathcal{P}} \Xi\{SSC_F(\mathbf{k} + p) \oplus SSC_M(\mathbf{l} + p)\}$$

References

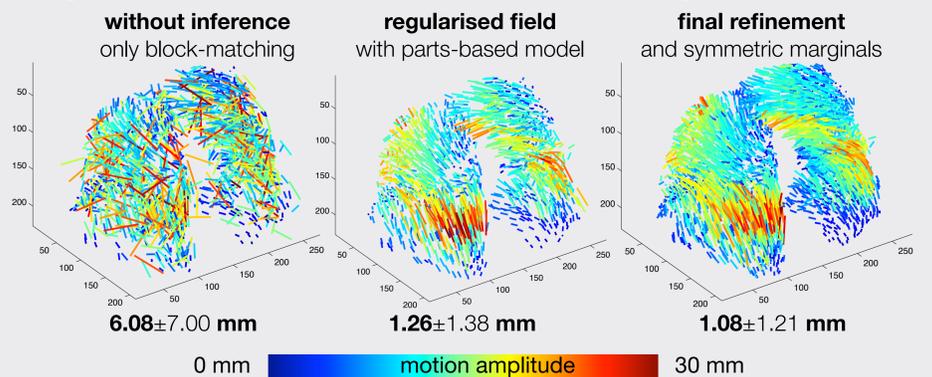
- [1] Heinrich et al.: "Towards realtime multimodal fusion ... using self-similarities", MICCAI (2013)
- [2] Felzenszwalb & Huttenlocher: "Pictorial structures for object recognition" IJCV (2005)
- [3] Castillo et al: "A reference dataset for deformable image registration ..." Phys. Med. Biol. (2013)

3. Parts-based model for regularisation

- Infer regularity over all displacement probabilities with MST model

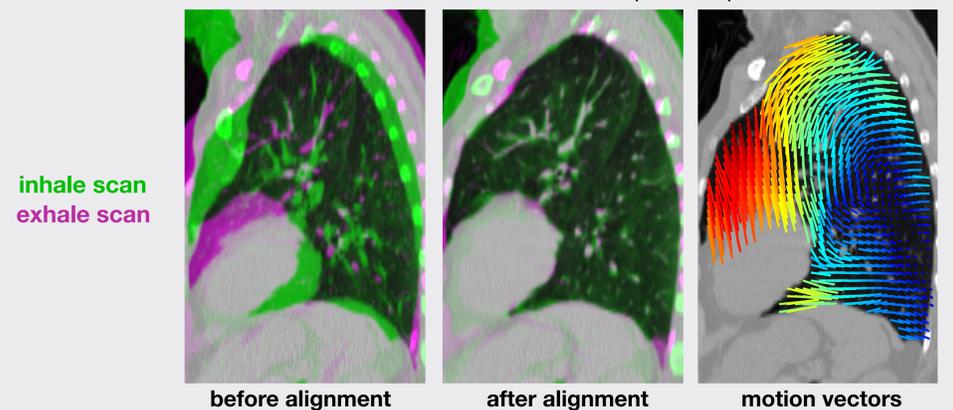
$$\mathcal{R}(\mathbf{d}_i, \mathbf{d}_j) = \frac{\|\mathbf{d}_i - \mathbf{d}_j\|^2}{\sqrt{\|\mathbf{x}_i - \mathbf{x}_j\|^2 + |I(\mathbf{x}_i) - I(\mathbf{x}_j)|/\sigma_I}}$$

- Regularisation and symmetry constraint improve registration drastically



Visual example of thin-plate spline fit

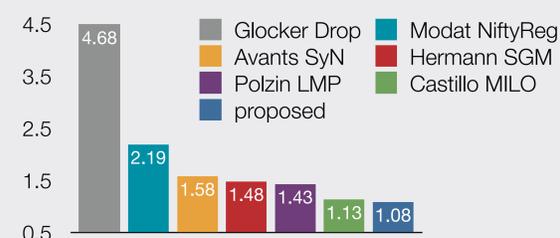
- Reconstructed dense motion field with thin-plate spline



- Overlay demonstrates well-aligned lung structures
- Diffeomorphisms cannot be directly guaranteed $std(Jac)=0.26$

Validation, Results and Comparison

- Evaluation on public COPDgene dataset of dir-lab.com [3]



fast run-time of ~2 min.
publicly available code:
mpheinrich.de/software.html

- Target registration error of **1.08mm** over 3000 landmarks

Outlook and Future Work

- Surface keypoints for (multi-modal) whole-body registration
- Remove topology-changing correspondences → diffeomorphisms
- Initialise any continuous registration tool with correspondence field

short oral presentation:

